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LA-UR--81-3735

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SUBMITTED TO International Workshop on Pion and Heavy Ion Radiotherapy,  
Vancouver, B.C., July 29-31, 1981

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## EFFECTS OF PIONS ON NORMAL TISSUES

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### INTRODUCTION

Pions, an intermediate-LET radiation, bear complex physical characteristics which depend on beam dimensions. For therapeutic application of pion beams, the Bragg peak must be spread out to encompass the treatment volume, and the range must be modulated to produce a uniform biological effect across the peak. The LET variation across the modulated peak must also be considered in terms of providing a uniform biological effect when fractionated schemes are employed. Verification of the uniform biological effectiveness of beams of various dimensions produced at LAMPF has been made using cultured mammalian cells<sup>1</sup> and mouse fibroblasts.<sup>2</sup> The latter is of more clinical relevance since fractionated doses of pions are used.

The contribution of charged particles and fast neutrons resulting from pion capture in tissue and the dependence of this contribution on pion treatment volume are together reported to be considered<sup>3</sup> and are discussed in detail in this workshop.<sup>4,5,6</sup> The role of fast neutrons becomes significant for larger pion treatment volumes. The volume-dependent RBE differences have been estimated by using cultured mammalian cells.<sup>7,8</sup> Our preliminary study using the mouse fibroblasts also indicates that fractionated treatment appears to result in a higher RBE value for large treatment volumes if the peak width remains the same.

In addition to the characterization of pion beams as a part of pretherapeutic radiobiology studies, RBE measurements in normal tissues, particularly for late effects, are of considerable importance since the normal tissue tolerance is often determined by the late effects.

In this paper, both the pre- and posttherapy ratios of LAMPF are reviewed with regard to (1) the dependence of fractionation on the therapy protocol and (2) the apparent ratio of late and acute effect during aging patients.

A brief historical characterisation of the therapy is given.

(1) Dependence of the late effect upon the size of the different peak penumbra.

MCU of water phantom were exposed to 1000-particle fraction of 0.1 Gy.

intervals between fractions) at the proximal and distal peak positions of a modulated 14 cm peak width beam (Fig. 1). Using the intestinal crypt survival assay as described by Withers and Elkind,<sup>7</sup> the results plotted as a function of the proximal peak dose indicated that the biological effects at both peak positions were similar (Fig. 2). This study confirmed that the modulation of the pion beam was appropriate.<sup>2</sup> It suggests that the RBE at the distal position is approximately 16% higher than at the proximal position.

(2) RBE variations for beams of small versus large peak width

A similar study was made to determine if variation in RBE exists for clinical beams of large (14 cm) or small (6 cm) peak width but having equal field size of 11 cm x 14 cm. Mice were given four pion dose fractions (3 hr intervals between fractions) at the mid peak position of the beams (Fig. 3). The intestinal crypt survival data showed no significant differences in biological effects for these two beams as shown in Fig. 4.

(3) Volume Effects

Two beams of an 8 cm peak width but of different field sizes, 7.5 cm x 7.5 cm or 20 cm x 20 cm (full width at half maximum), were tested using the mouse jejunum for one and four pion dose fractions given at the mid peak position.

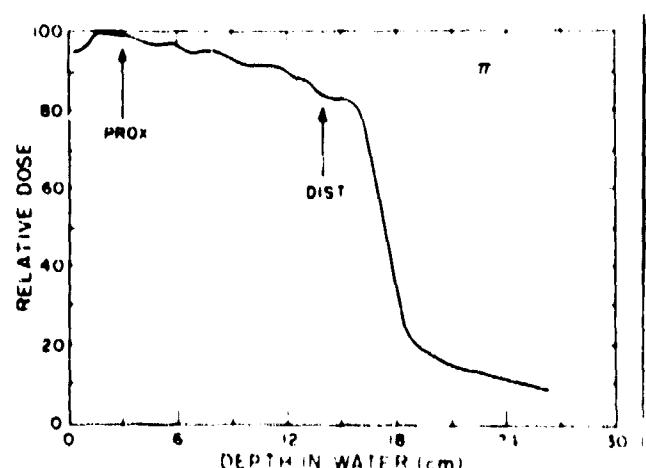


Fig. 1. Dose distribution curve of a 14 cm peak width beam in a water phantom. The beam size was 11 cm x 14 cm. The arrows indicate the positions at which mice were exposed to pions. Note that the distal peak dose is approximately 16% less than the proximal dose (Figure modified from ref. 2).

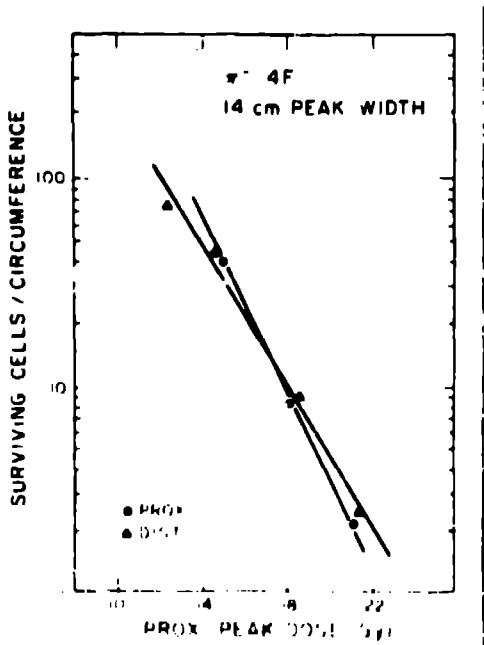


FIG. 2 The intestinal crypt cell survivals for 4 pion dose fractions expressed as a function of the proximal peak dose (Figure modified from Ref. 7).

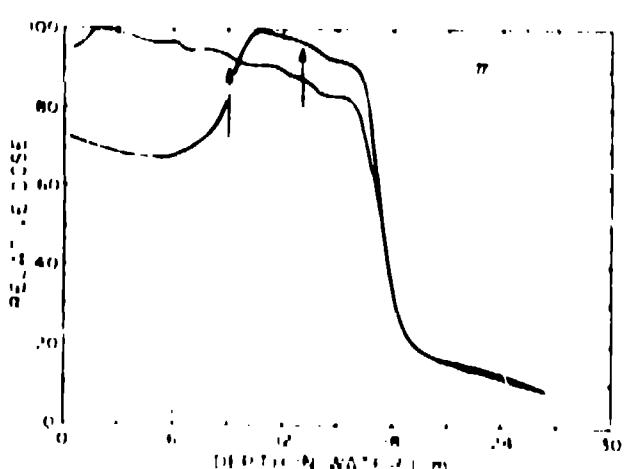


FIG. 3 The distribution of a proton beam with a 14 cm peak width with an equivalent uniform dose of 16 Gy. The arrows indicate the positions at which doses were expected to have changed (modified from Ref. 2).

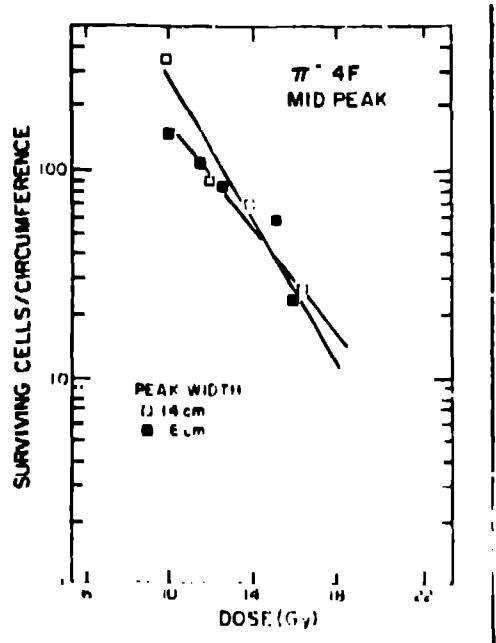


Fig. 4. The intestinal crypt cell survivals for 4 pion dose fractions expressed as a function of the dose for the two beams of different peak width which are described in Fig. 3 (Figure modified from Ref. 2).

The dose rate was  $0.1-0.12$  Gy/min for the large beam and  $0.6$  Gy/min for the small beam. Our preliminary data indicate that at four fractions, the biological effect is greater for the large beam compared to the small beam despite the fact that the dose rate for the large beam is considerably lower than that for the small beam. No differences in biological effects, however, are observed at single fractions as shown in Fig. 5.

#### B. RBE Measurements

RBE measurements with pions for various normal tissues at LAMIE have, so far, been made using beams with narrow peak widths because of limited dose rate in the past. The RBE values of such beams may be different from beams used clinically due to differences in LET, thus limiting the use of such data for the clinical problem. The RBE data available to date were compiled for acute effects on mouse skin,<sup>8</sup> mouse jejunum,<sup>9,10</sup> and for late effects on the mouse kidney,<sup>11</sup> rat spinal cord,<sup>12</sup> and rat colon<sup>13</sup> as shown in Figs. 6 and Table I. The RBE values are, in general, best-fitted by a power function when the RBE is plotted as a function of dose per fraction. The slopes for late

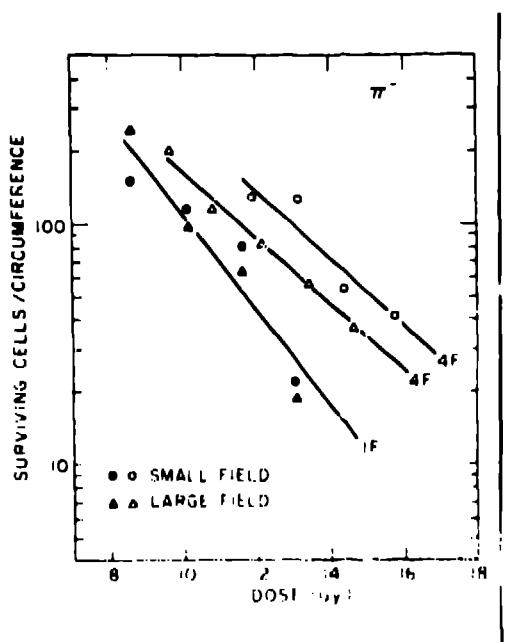


Fig. 5. Effect of beams of 8 cm peak width but different field sizes ( $7.5 \text{ cm} \times 7.5 \text{ cm}$  and  $20 \text{ cm} \times 20 \text{ cm}$ ) on survival of intestinal crypt cells following 1 and 4 pion dose fractions.

TABLE I  
PARAMETERS FOR RBE VALUES EXPRESSED AS A FUNCTION OF DOSE PER FRACTION

Tissue	Dose (Rads)	RBE = $R_D^{1/2}$	$\alpha$	$\beta$	Ref.
Skin	3 cm	1.97	0.20		(8)
Jejunum	3 cm	1.08	0.34		(9)
Jejunum	4 cm	1.41	0.12		(10)
Jejunum	14 cm	1.04	0.77		(2)
Kidney	1 cm	1.86	0.31		(11)
Spinal Cord	2 cm	1.19	0.41		(12)
Colon	2 cm	1.66	0.38		(13)

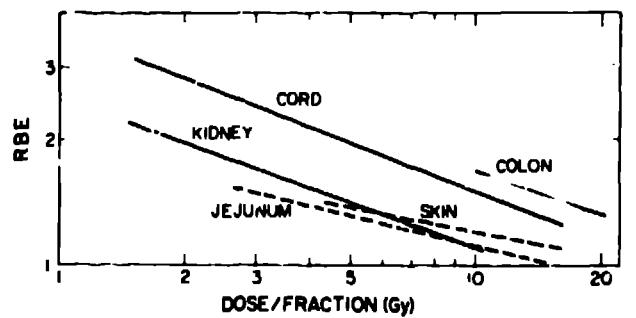


Fig. 6. RBE values plotted as a function of dose per fraction. Solid lines for late effects and dotted lines for acute effects. Sources: Skin, Jejunum, Kidney, Spinal Cord, and Colon.

effects appear to be steeper compared to those for acute effects. For example, at clinically relevant dose fraction regions, the RBE value for the jejunum (acute effect) is considerably less than that for the spinal cord (late effect).

When the values for repair per low fraction (fractional repair) were compared, the data suggest that the fractional repair is considerably faster for protons compared to X-rays regardless of tissue studied (Table 1). Further, the fractional repair ratios (proton/X-ray) also appear to vary dependent on tissue, fraction number as well as beam type. At five fractions, the ratio for mouse skin, for example, is 0.56 ± 0.11 and that for jejunum is 0.77 ± 0.04. As the number of fractions increases, the fractional repair for late effects seems to decrease, whereas, that for the kidney late effect appears to increase.

#### DISCUSSION

Preliminary radiobiology studies resulting from laboratory programs are beginning to clarify the uniformity of biological effect across the many proton facilities around the world of various dimensions and capabilities for acute and late effects of proton therapy. The results of these large clinical beam types often translate well to the clinic, provided that the appropriate experimental system (since the exposure conditions do not affect the final outcome) and the field size are used to match the quality of radiation. In addition, it will be important to consider the field of the body of the animal, the effect of scatter, as well as the location of mouth also to be taken into consideration.

TABLE 2  
COMPARISON OF FRACTIONAL REPAIR VALUES<sup>a</sup> FOR X RAYS AND PIONS

Tissues	Number of Fractions					Ref.
	2F	4F	5F	10F	15F	
Skin	X 0.59 Pi 0.39			0.57 0.37		(8)
Colon	X 0.45 Pi 0.19			0.52 0.19		(9)
Esophagus	X 0.36 Pi 0.11	0.36 0.11		0.44 0.19		(10)
Esophagus	X 0.32 Pi 0.19	0.32 0.19				(11)
Kidney	X 0.41 Pi 0.17		0.41 0.17		0.45 0.17	(12)
Ovarian tumor	X 0.36 Pi 0.17		0.36 0.17		0.36 0.17	(13)
Uterus	X 0.41 Pi 0.22					

<sup>a</sup> The fractional repair value expressed as  $D_{100}/D_{100}^{\text{X}}$ , where  $D_{100}$  is the dose required to produce 100% survival and  $D_{100}^{\text{X}}$  is the dose required to produce 100% survival by X rays.

A comprehensive review of previous literature has been reported previously.<sup>14</sup> In our studies of pion therapy, many fractionated irradiation with pion beams resulted in greater than 100% survival compared to the same effect with the pions. This therapeutic effect appears to result from the dose delivered per fraction. Our experiments are presented in the third thermom.

In the first of the three experiments, we studied evidence of late effects on the skin of the rat. After a single dose of 100 rad treatment with a 100 MeV pion beam, no late effects were observed. Late effects, however, did appear after a series of 10 fractions of 100 rad each. We believe that the late effects observed in this experiment were due to the dose per fraction being greater than the dose per fraction in the first experiment. These results are presented in the fourth thermom.

tissues, particularly for late effects, are required to obtain a better understanding of optimal pion fractionation schemes. Such efforts on the late effect studies of normal tissues (spinal cord, lung, kidney, liver, colon and lens in rodents) are in progress through collaborations at Los Alamos.

#### ACKNOWLEDGEMENTS

The author is grateful to Drs. L. D. Skarpgard, M. R. Raju, R. A. Tobey and A. J. van der Kogel for their comments and advice during the preparation of the text and to Marla Griffith for typing this manuscript.

This investigation was supported by the Grant CA17236 awarded by the U.S. National Cancer Institute, NIH and by DOE.

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